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# Motion microscopy for visualizing and quantifying small motions

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Although the human visual system is remarkable at perceiving and interpreting motions, it has limited sensitivity, and we cannot see motions that are smaller than some threshold. Although difficult to visualize, tiny motions below this threshold are important and can reveal physical mechanisms, or be precursors to large motions in the case of mechanical failure. Here, we present a “motion microscope,” a computational tool that quantifies tiny motions in videos and then visualizes them by producing a new video in which the motions are made large enough to see. Three scientific visualizations are shown, spanning macroscopic to nanoscopic length scales. They are the resonant vibrations of a bridge demonstrating simultaneous spatial and temporal modal analysis, micrometer vibrations of a metamaterial demonstrating wave propagation through an elastic matrix with embedded resonating units, and nanometer motions of an extracellular tissue found in the inner ear demonstrating a mechanism of frequency separation in hearing. In these instances, the motion microscope uncovers hidden dynamics over a variety of length scales, leading to the discovery of previously unknown phenomena.

visualization | motion | image processing

**M**otion microscopy is a computational technique to visualize and analyze meaningful but small motions. The motion microscope enables the inspection of tiny motions as optical microscopy enables the inspection of tiny forms. We demonstrate its utility in three disparate problems from biology and engineering: visualizing motions used in mammalian hearing, showing vibration modes of structures, and verifying the effectiveness of designed metamaterials.

The motion microscope is based on video magnification (1–4), which processes videos to amplify small motions of any kind in a specified temporal frequency band. We extend the visualization produced by video magnification to scientific and engineering analysis. In addition to visualizing tiny motions, we quantify both the object’s subpixel motions and the errors introduced by camera sensor noise (5). Thus, the user can see the magnified motions and obtain their values, with variances, allowing for both qualitative and quantitative analyses.

The motion microscope characterizes and amplifies tiny local displacements in a video by using spatial local phase. It does this by transforming the captured intensities of each frame’s pixels into a wavelet-like representation where displacements are represented by phase shifts of windowed complex sine waves. The representation is the complex steerable pyramid (6), an over-complete linear wavelet transform, similar to a spatially localized Fourier transform. The transformed image is a sum of basis functions, approximated by windowed sinusoids (Fig. S1), that are simultaneously localized in spatial location  $(x, y)$ , scale  $r$ , and orientation  $\theta$ . Each basis function coefficient gives spatially

local frequency information and has an amplitude  $A_{r,\theta}(x, y)$  and a phase  $\phi_{r,\theta}(x, y)$ .

To amplify motions, we compute the unwrapped phase difference of each coefficient of the transformed image at time  $t$  from its corresponding value in the first frame,

$$\Delta\phi_{r,\theta}(x, y, t) := \phi_{r,\theta}(x, y, t) - \phi_{r,\theta}(x, y, 0). \quad [1]$$

We isolate motions of interest and remove components due to noise by temporally and spatially filtering  $\Delta\phi_{r,\theta}$ . We amplify the filtered phase shifts by the desired motion magnification factor to obtain modified phases for each basis function at each time  $t$ . We then transform back each frame’s steerable pyramid to produce the motion-magnified output video (Fig. S2) (3).

We estimate motions under the assumption that there is a single, small motion at each spatial location. In this case, each coefficient’s phase difference,  $\Delta\phi_{r,\theta}$ , is approximately equal to the dot product of the corresponding basis function’s orientation and the 2D motion (7) (*Relation Between Local Phase Differences and Motions*). The reliability of spatial local phase varies across scale and orientations, in direct proportion to the coefficient’s amplitude (e.g., coefficients for basis functions orthogonal to an edge are more reliable than those along it) (Fig. S3 and

## Significance

Humans have difficulty seeing small motions with amplitudes below a threshold. Although there are optical techniques to visualize small static physical features (e.g., microscopes), visualization of small dynamic motions is extremely difficult. Here, we introduce a visualization tool, the motion microscope, that makes it possible to see and understand important biological and physical modes of motion. The motion microscope amplifies motions in a captured video sequence by rerendering small motions to make them large enough to see and quantifies those motions for analysis. Amplification of these tiny motions involves careful noise analysis to avoid the amplification of spurious signals. In the representative examples presented in this study, the visualizations reveal important motions that are invisible to the naked eye.

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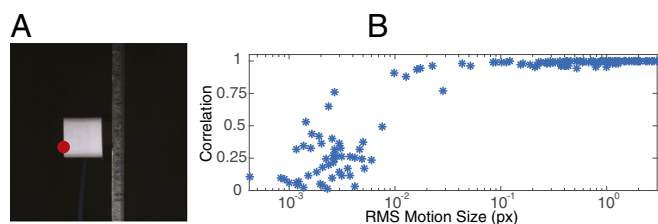
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**Fig. 1.** A comparison of our quantitative motion estimation vs. a laser vibrometer. Several videos of a cantilevered beam excited by a shaker were taken with varying focal length, exposure times, and excitation magnitude. The horizontal, lateral motion of the red point was also measured with a laser vibrometer. (A) A frame from one video. (B) The correlation between the two signals across the videos vs. root mean square (RMS) motion size in pixels (px). Only motions at the red point in A were used in our analysis. More results are in Fig. S4.

*Low-Amplitude Coefficients Have Noisy Phase*). We combine information about the motion from multiple orientations by solving a weighted least squares problem with weights equal to the amplitude squared. The result is a 2D motion field. This processing is accurate, and we provide comparisons to other algorithms and sensors (Fig. 1, *Synthetic Validation*, and Figs. S4 and S5).

For a still camera, the sensitivity of the motion microscope is mostly limited by local contrast and camera noise—fluctuations of pixel intensities present in all videos (5). When the video is motion-magnified, this noise can lead to spurious motions, especially at low-contrast edges and textures (Fig. S6). We measure motion noise level by computing the covariance matrix of each estimated motion vector. Estimating this directly from the input video is usually impossible, because it requires observing the motions without noise. We solve this by creating a simulated noisy video with zero motion, replicating a static frame of the input video and adding realistic, independent noise to

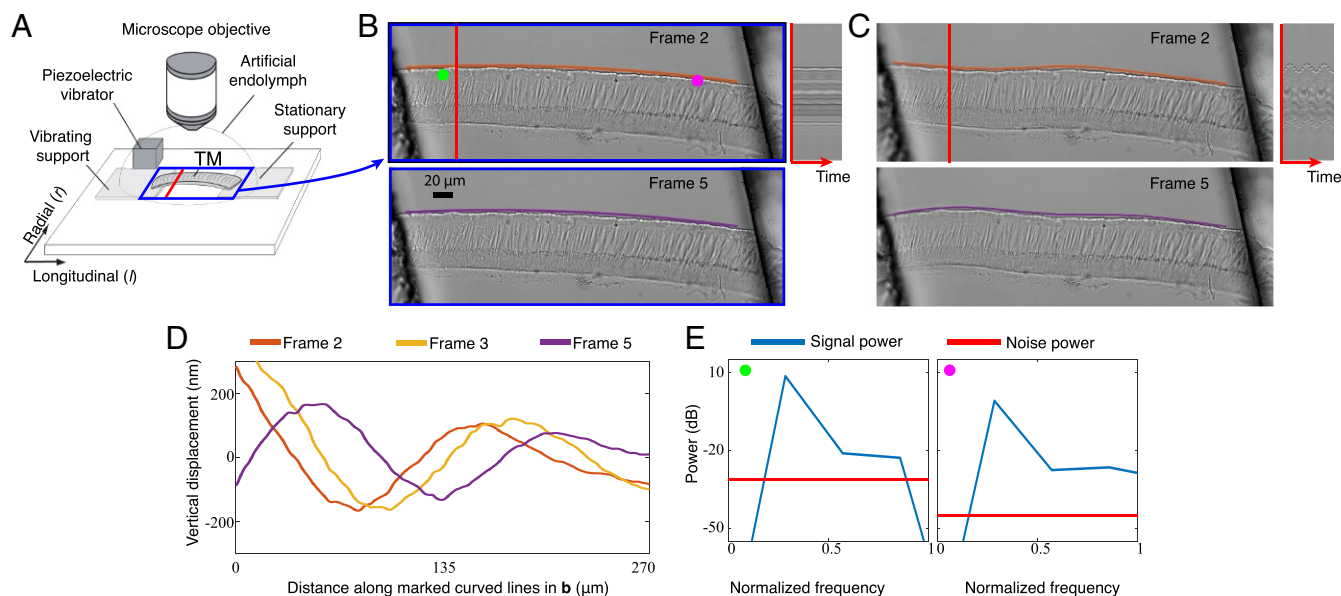
each frame. We compute the sample covariance of the estimated motion vectors in this simulated video (Fig. S7 and *Noise Model and Creating Synthetic Video*). We show analytically, and via experiments in which the motions in a temporal band are known to be zero, that these covariance matrices are accurate for real videos (*Analytic Justification of Noise Analysis* and Figs. S8 and S9). We also analyze the limits of our technique by comparing to a laser vibrometer and show that, with a Phantom V-10 camera, at a high-contrast edge, the smallest motion we can detect is on the order of 1/100th of a pixel (Fig. 1 and Fig. S4).

## Results and Discussion

We applied the motion microscope to several problems in biology and engineering. First, we used it to reveal one component of the mechanics of hearing. The mammalian cochlea is a remarkable sensor that can perform high-quality spectral analysis to discriminate as many as 30 frequencies in the interval of a semitone (8). These extraordinary properties of the hearing organ depend on traveling waves of motion that propagate along the cochlear spiral. These wave motions are coupled to the extremely sensitive sensory receptor cells via the tectorial membrane, a gelatinous structure that is 97% water (9).

To better understand the functional role of the tectorial membrane in hearing, we excised segments of the tectorial membrane from a mouse cochlea and stimulated it with audio frequency vibrations (Movie S1 and Fig. 2A). Prior work suggested that motions of the tectorial membrane would rapidly decay with distance from the point of stimulation (10). The unprocessed video of the tectorial membrane appeared static, making it difficult to verify this. However, when the motions were amplified 20 times, waves that persisted over hundreds of micrometers were revealed (Movie S1 and Fig. 2B–E).

Subpixel motion analysis suggests that these waves play a prominent role in determining the sensitivity and frequency selectivity of hearing (11–14). Magnifying motions has provided new insights into the underlying physical mechanisms of hearing.



**Fig. 2.** Exploring the mechanical properties of a mammalian tectorial membrane with the motion microscope. (A) The experimental setup used to stroboscopically film a stimulated mammalian tectorial membrane (*Tecta*<sup>Y1870C/+</sup>). Subfigure Copyright (2007) National Academy of Sciences of the United States of America. Reproduced from ref. 12. (B) Two of the eight captured frames. (Movie S1, data previously published in ref. 13). (C) Corresponding frames from the motion-magnified video in which displacement from the mean was magnified 20×. The orange and purple lines on top of the tectorial membrane in B are warped according to magnified motion vectors to produce the orange and purple lines in C. (D) The vertical displacement along the orange and purple lines in B is shown for three frames. (E) The power spectrum of the motion signal and noise power is shown in the direction of least variance at the magenta and green points in B.

Ultimately, the motion microscope could be applied to see and interpret the nanoscale motions of a multitude of biological systems.

We also applied the motion microscope to the field of modal analysis, in which a structure's resonant frequencies and mode shapes are measured to characterize its dynamic behavior (15). Common applications are to validate finite element models and to detect changes or damage in structures (16). Typically, this is done by measuring vibrations at many different locations on the structure in response to a known input excitation. However, approximate measurements can be made under operational conditions assuming broadband excitation (17). Contact accelerometers have been traditionally used for modal analysis, but densely instrumenting a structure can be difficult and tedious, and, for light structures, the accelerometers' mass can affect the measurement.

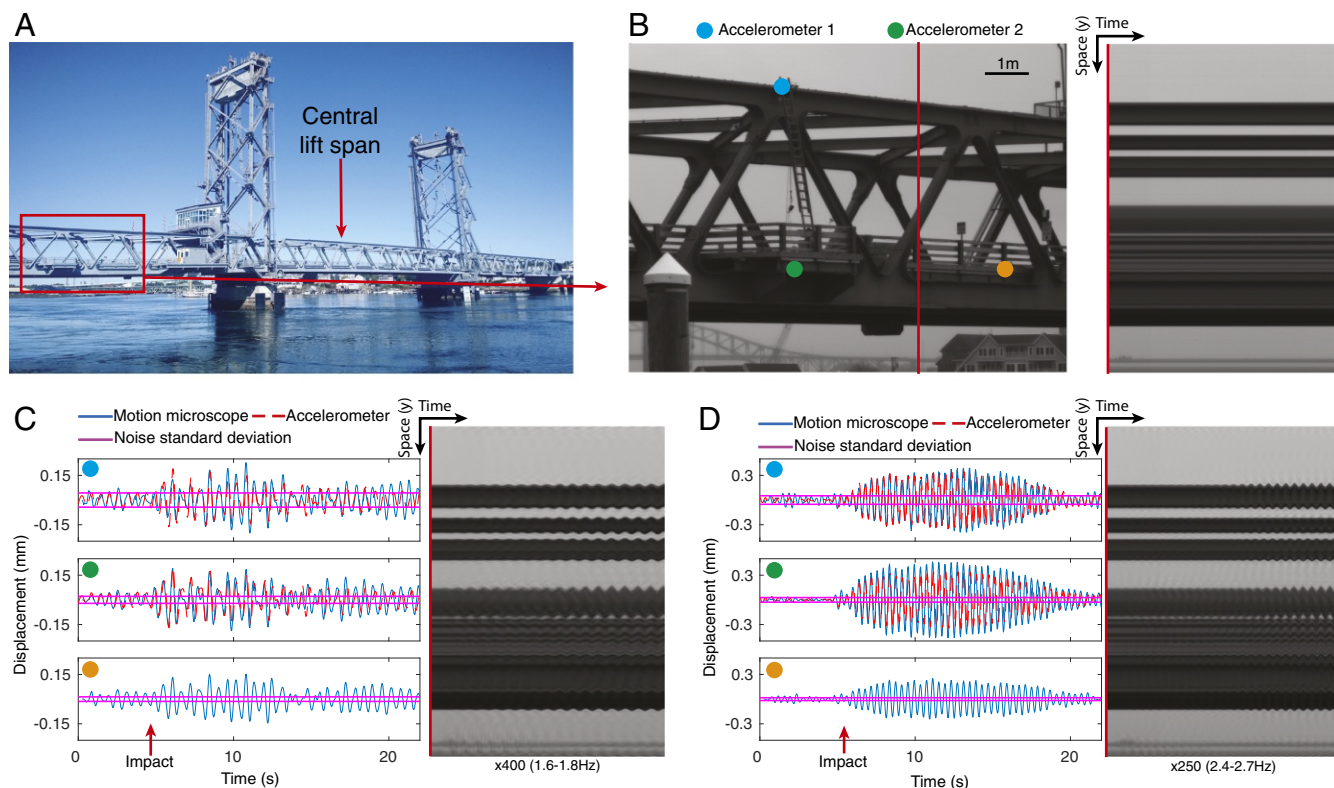
The motion microscope offers many advantages over traditional sensors. The structure is unaltered by the measurement, the measurements are spatially dense, and the motion-magnified video allows for easy interpretation of the motions. While only structural motions in the image plane are visible, this can be mitigated by choosing the viewpoint carefully.

We applied the motion microscope to modal analysis by filming the left span of a suspension bridge from 80 m away (Fig. 3A). The central span was lowered and impacted the left span. Despite this, the left span looks completely still in the input video (Fig. 3B). Two of its modal shapes are revealed in [Movie S2](#) when magnified  $400\times$  (1.6 Hz to 1.8 Hz) and  $250\times$  (2.4 Hz to 2.7 Hz). In Fig. 3C and D, we show time slices from the motion-magnified videos, displacements versus time at three points, and the estimated noise standard deviations. We also used accelerometers

to measure the motions of the bridge at two of those points (Fig. 3B). The motion microscope matches the accelerometers within error bars. In a second example, we show the modal shapes of a pipe after it is struck with a hammer (*Modal Shapes of a Pipe*, Fig. S10, and Movie S3).

In our final example, we used the motion microscope to verify the functioning of elastic metamaterials, artificially structured materials designed to manipulate and control the propagation of elastic waves. They have received much attention (18) because of both their rich physics and their potential applications, which include wave guiding (19), cloaking (20), acoustic imaging (21), and noise reduction (22). Several efforts have been made to experimentally characterize the elastic wave phenomena observed in these systems. However, as the small amplitude of the propagating waves makes it impossible to directly visualize them, the majority of the experimental investigations have focused on capturing the band gaps through the use of accelerometers, which only provide point measurements. Visualizing the mechanical motions everywhere in the metamaterials has only been possible using expensive and highly specialized setups like scanning laser vibrometers (23).

We focus on a metamaterial comprising an elastic matrix with embedded resonating units, which consists of copper cores connected to four elastic beams (24). Even when vibrated, this metamaterial appears stationary, making it difficult to determine if the metamaterial is functioning correctly (Movies S4 and S5). Previously, these miniscule vibrations were measured with two accelerometers (24). This method only provides point measurements, making it difficult to verify the successful attenuation of vibrations. We gain insight and understanding of the system by visually amplifying its motion.



**Fig. 3.** The motion microscope reveals modal shapes of a lift bridge. (A) The outer spans of the bridge are fixed while the central span moves vertically. (B) The left span was filmed while the central span was lowered. A frame from the resulting video and a time slice at the red line are shown. (C) Displacement and noise SD from the motion microscope are shown for motions in a 1.6- to 1.8-Hz band at the cyan, green, and orange points in B. Doubly integrated data from accelerometers at the cyan and green points are also shown. A time slice from the motion-magnified video is shown (Movie S2). The time at which the central span is fully lowered is marked as “impact.” (D) Same as C, but for motions in a 2.4- to 2.7-Hz band.





We used our motion estimation method to compute the horizontal displacement of the marked, red point on the left side of the accelerometer from the video (Fig. 1A). We applied a temporal band-stop filter to remove motions between 67 Hz and 80 Hz that corresponded to camera motions caused by its cooling fan's rotation. The laser vibrometer signal was integrated using discrete, trapezoidal integration. Before integration, both signals were high-passed above 2.5 Hz to reduce low-frequency noise in the integrated vibrometer signal. The motion signals from each video were manually aligned. For one video (exposure, 490  $\mu$ s; excitation, 25; and focal length, 85 mm), we plot the two motion signals (Fig. S4 B–D). They agree remarkably well, with higher modes well aligned and a correlation of 0.997.

To show the sensitivity of the motion microscope, we plot the correlation of our motion estimate and the integrated velocities from the laser vibrometer vs. motion size (RMS displacement). Because the motion's average size varies over time, we divide each video's motion signal into eight equal pieces and plot the correlations of each piece in each video in Fig. S4 E and F. For RMS displacements on the order of 1/100th of a pixel, the correlation between the two signals varies between 0.87 and 0.94. For motions larger than 1/20th of a pixel, the correlation is between 0.95 and 0.999. Possible sources of discrepancy are noise in the motion microscope signal, integrated low-frequency noise in the vibrometer signal, and slight misalignment between the signals. Displacements with RMS smaller than 1/100th of a pixel were noisier and had lower correlations, indicating that noise in the video prevents the two signals from matching.

As expected, correlation increases with focal length and excitation magnitude, two things that positively correlate with motion size (in pixels) (Fig. S4 G and H). The correlation also increases with exposure, because videos with lower exposure times are noisier (Fig. S4I).

**Filming Bridge Sequence.** The bridge was filmed with a monochrome Point Gray Grasshopper3 camera (model GS3-U3-2356M-C) at 30 FPS with a resolution of 800  $\times$  600. The central span of the bridge lifted to accommodate marine traffic. Filming was started about 5 s before the central span was lowered to its lowest point.

The accelerometer data were doubly integrated using trapezoidal integration to displacement. In Fig. 3 C and D, both the motion microscope displacement and the doubly integrated acceleration were band-passed with a first-order band-pass Butterworth filter with the specified parameters.

**Motion Field Interpolation.** In textureless regions, it may not be possible to estimate the motion at all, and, at one-dimensional structures like edges, the motion field will only be accurate in the direction perpendicular to the edge. These inaccuracies are reflected in the motion covariance matrix. We show how to interpolate the motion field from accurate regions to inaccurate regions, assuming that adjacent pixels have similar motions.

We minimize the following objective function:

$$\sum_{\mathbf{x}} (\mathbf{V}_S(\mathbf{x}) - \mathbf{V}(\mathbf{x})) \Sigma_V^{-1}(\mathbf{x}) (\mathbf{V}_S(\mathbf{x}) - \mathbf{V}(\mathbf{x}))^T + \lambda_S \sum_{\mathbf{y} \in \mathcal{N}(\mathbf{x})} (\mathbf{V}_S(\mathbf{x}) - \mathbf{V}_S(\mathbf{y})) (\mathbf{V}_S(\mathbf{x}) - \mathbf{V}_S(\mathbf{y}))^T, \quad [6]$$

where  $\mathbf{V}_S$  is the desired interpolated field,  $\mathbf{V}$  is the estimated motion field,  $\Sigma_V$  is its covariance,  $\mathcal{N}(\mathbf{x})$  is the four-pixel neighborhood of  $\mathbf{x}$ , and  $\lambda_S$  is a user-specified constant that specifies the relative importance of matching the estimated motion field vs. making adjacent pixels have similar motion fields. The first term seeks to ensure that  $\mathbf{V}_S$  is close to  $\mathbf{V}$ , weighted by the expected amount of noise at each pixel. The second term seeks to ensure that adjacent pixels have similar motion fields.

In Fig. 4D, we produce the color overlays by applying the above processing to the estimated motion field with  $\lambda_S = 300$  and then taking the amplitude of each motion vector. We also set components of the covariance matrix that were larger than 0.1 square pixels to be an arbitrarily large number (we used 10,000 square pixels).

**Finite Element Analysis of Acoustic Metamaterial.** We use Abaqus/Standard (29), a commercial finite-element analyzer, to simulate the metamaterial's response to forcing. We constructed a 2D model with 37,660 nodes and 11,809 eight-node plane strain quadrilateral elements (Abaqus element type CPE8H). We modeled the rubber as Neo-Hookean, with shear modulus 443.4 kPa, bulk modulus  $7.39 \times 10^5$  kPa, and density 1,050 kg·m<sup>3</sup> (Abaqus parameters C10 = 221.7 kPa, D1 =  $2.71 \times 10^{-9}$  Pa<sup>-1</sup>). We modeled the copper core with shear modulus  $4.78 \times 10^7$  kPa, bulk modulus  $1.33 \times 10^8$  kPa, and density 8,960 kg·m<sup>3</sup> (Abaqus parameters C10 =  $2.39 \times 10^7$  kPa, D1 =  $1.5 \times 10^{-11}$  Pa<sup>-1</sup>). Geometry and material properties are specified in Wang et al. (24). The bottom of the metamaterial was given a zero-displacement boundary condition. A sinusoidal displacement loading condition at the forcing frequency was applied to a node located halfway between the top and bottom of the metamaterial.

**Validation of Noise Analysis with Real Video Data.** We took a video of an accelerometer attached to a beam (Fig. S9A). We used the accelerometer to verify that the beam had no motions between 600 Hz and 700 Hz (Fig. S9B). We then estimated the in-band motions from a video of the beam. Because the beam is stationary in this band, these motions are entirely due to noise, and their temporal sample covariance gives us a ground-truth measure of the noise level (Fig. S9C). We used our simulation with a signal-dependent noise model to estimate the covariance matrix from the first frame of the video, the specific parameters of which are shown in Fig. S9D. The resulting covariance matrices closely match the ground truth (Fig. S9 E and F), showing that our simulation can accurately estimate noise level and error bars.

We also verify that the signal-dependent noise model performs better than the simpler constant variance noise model, in which noise is IID. The result of the constant noise model simulation produced results that are much less accurate than the signal-dependent noise model (Fig. S9 G and H).

In Fig. S9, we only show the component of the covariance matrix corresponding to the direction of least variance, and only at points corresponding to edges or corners.

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- Liu C, Torralba A, Freeman WT, Durand F, Adelson EH (2005) Motion magnification. *ACM Trans Graph* 24:519–526.
- Wu HY, et al. (2012) Eulerian video magnification for revealing subtle changes in the world. *ACM Trans Graph* 31:1–8.
- Wadhwa N, Rubinstein M, Durand F, Freeman WT (2013) Phase-based video motion processing. *ACM Trans Graph* 32:80.
- Wadhwa N, Rubinstein M, Durand F, Freeman WT (2014) Riesz pyramid for fast phase-based video magnification. *IEEE International Conference on Computational Photography* (Inst Electr Electron Eng, New York), pp 1–10.
- Nakamura J (2005) *Image Sensors and Signal Processing for Digital Still Cameras* (CRC, Boca Raton, FL).
- Simoncelli EP, Freeman WT (1995) The steerable pyramid: A flexible architecture for multi-scale derivative computation. *Int J Image Proc* 3:444–447.
- Fleet DJ, Jepson AD (1990) Computation of component image velocity from local phase information. *Int J Comput Vis* 5:77–104.
- Dallos P, Fay RR (2012) *The Cochlea*, Springer Handbook of Auditory Research (Springer Science, New York), Vol 8.
- Thalmann I (1993) Collagen of accessory structures of organ of Corti. *Connect Tissue Res* 29:191–201.
- Zwislocki JJ (1980) Five decades of research on cochlear mechanics. *J Acoust Soc Am* 67:1679–1685.
- Sellon JB, Farrahi S, Ghaffari R, Freeman DM (2015) Longitudinal spread of mechanical excitation through tectorial membrane traveling waves. *Proc Natl Acad Sci USA* 112:12968–12973.
- Ghaffari R, Aranyosi AJ, Freeman DM (2007) Longitudinally propagating traveling waves of the mammalian tectorial membrane. *Proc Natl Acad Sci USA* 104:16510–16515.
- Sellon JB, Ghaffari R, Farrahi S, Richardson GP, Freeman DM (2014) Porosity controls spread of excitation in tectorial membrane traveling waves. *J Biophys* 106:1406–1413.
- Ghaffari R, Aranyosi AJ, Richardson GP, Freeman DM (2010) Tectorial membrane traveling waves underlie abnormal hearing in tectb mutants. *Nat Commun* 1:96.
- Ewins DJ (1995) *Modal Testing: Theory and Practice*, Engineering Dynamics Series (Res Stud, Baldock, UK) Vol 6.
- Salawu O (1997) Detection of structural damage through changes in frequency: A review. *Eng Struct* 19:718–723.
- Hermans L, van der Auweraer H (1999) Modal testing and analysis of structures under operational conditions: Industrial applications. *Mech Sys Signal Process* 13:193–216.
- Hussein MI, Leamy MJ, Ruzzene M (2014) Dynamics of phononic materials and structures: Historical origins, recent progress, and future outlook. *Appl Mech Rev* 66:040802.
- Khelif A, Choujaa A, Benchabane S, Djafari-Rouhani B, Laude V (2004) Guiding and bending of acoustic waves in highly confined phononic crystal waveguides. *Appl Phys Lett* 84:4400–4402.

20. Cummer S, Schurig D (2007) One path to acoustic cloaking. *New J Phys* 9:45.
21. Spadoni A, Daraio C (2010) Generation and control of sound bullets with a nonlinear acoustic lens. *Proc Natl Acad Sci USA* 107:7230–7234.
22. Elser D, et al. (2006) Reduction of guided acoustic wave Brillouin scattering in photonic crystal fibers. *Phys Rev Lett* 97:133901.
23. Jeong S, Ruzzene M (2005) Experimental analysis of wave propagation in periodic grid-like structures. *Proc SPIE* 5760:518–525.
24. Wang P, Casadei F, Shan S, Weaver JC, Bertoldi K (2014) Harnessing buckling to design tunable locally resonant acoustic metamaterials. *Phys Rev Lett* 113: 014301.
25. Portilla J, Simoncelli EP (2000) A parametric texture model based on joint statistics of complex wavelet coefficients. *Int J Comput Vis* 40:49–70.
26. Liu C, Freeman WT, Szeliski R, Kang SB (2006) Noise estimation from a single image. *2006 IEEE Computer Society Conference on Computer Vision and Pattern Recognition* (Inst Electr Electron Eng, New York), pp 901–908.
27. Oppenheim AV, Schaffer RW (2010) *Discrete-Time Signal Processing* (Prentice Hall, New York).
28. Durst F, Melling A, Whitelaw JH (1976) *Principles and Practice of Laser-Doppler Anemometry*. NASA STI/Recon Technical Report A (NASA, Washington, DC), Vol 76.
29. Hibbitt, Karlsson, Sorensen (1998) *ABAQUS/Standard: User's Manual* (Hibbitt, Karlsson & Sorensen, Pawtucket, RI) Vol 1.
30. Blaber J, Adair B, Antoniou A (2015) Ncorr: Open-source 2D digital image correlation MATLAB software. *Exp Mech* 55:1105–1122.
31. Xu J, Moussawi A, Gras R, Lubineau G (2015) Using image gradients to improve robustness of digital image correlation to non-uniform illumination: Effects of weighting and normalization choices. *Exp Mech* 55:963–979.
32. Unser M (1999) Splines: A perfect fit for signal and image processing. *Signal Process Mag* 16:22–38.
33. Fleet DJ (1992) *Measurement of Image Velocity* (Kluwer Acad, Norwell, MA).
34. Hasinoff SW, Durand F, Freeman WT (2010) Noise-optimal capture for high dynamic range photography. *2010 IEEE Computer Society Conference on Computer Vision and Pattern Recognition* (Inst Electr Electron Eng, New York), pp 553–560.
35. Lucas BD, Kanade T (1981) An iterative image registration technique with an application to stereo vision. *Int Joint Conf Artif Intell* 81:674–679.
36. Horn B, Schunck B (1981) Determining optical flow. *Artif Intell* 17:185–203.
37. Wadhwa N, et al. (2016) Eulerian video magnification and analysis. *Commun ACM* 60:87–95.
38. Wachel JC, Morton SJ, Atkins KE (1990) Piping vibration analysis. *Proceedings of the 19th Turbomachinery Symposium*, pp 119–134.